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REVIEW

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Upper limb kinematics after cervical spinal cord injury: a review

Sébastien Mateo^{1,2,3,5*}, Agnès Roby-Brami⁴, Karen T Reilly¹, Yves Rossetti^{1,2}, Christian Collet³ and Gilles Rode^{1,2,5}

Abstract

Although a number of upper limb kinematic studies have been conducted, no review actually addresses the key-features of open-chain upper limb movements after cervical spinal cord injury (SCI). The aim of this literature review is to provide a clear understanding of motor control and kinematic changes during open-chain upper limb reaching, reach-to-grasp, overhead movements, and fast elbow flexion movements after tetraplegia. Using data from MEDLINE between 1966 and December 2014, we examined temporal and spatial kinematic measures and when available electromyographic recordings. We included fifteen control case and three series case studies with a total of 164 SCI participants and 131 healthy control participants. SCI participants efficiently performed a broad range of tasks with their upper limb and movements were planned and executed with strong kinematic invariants like movement endpoint accuracy and minimal cost. Our review revealed that elbow extension without *triceps brachii* relies on increased scapulothoracic and glenohumeral movements providing a dynamic coupling between shoulder and elbow. Furthermore, contrary to normal grasping patterns where grasping is prepared during the transport phase, reaching and grasping are performed successively after SCI. The prolonged transport phase ensures correct hand placement while the grasping relies on wrist extension eliciting either whole hand or lateral grip. One of the main kinematic characteristics observed after tetraplegia is motor slowing attested by increased movement time. This could be caused by (i) decreased strength, (ii) *triceps brachii* paralysis which disrupts normal agonist-antagonist co-contractions, (iii) accuracy preservation at movement endpoint, and/or (iv) grasping relying on tenodesis. Another feature is a reduction of maximal superior reaching during overhead movements which could be caused by i) strength deficit in agonist muscles like *pectoralis major*, ii) strength deficit in proximal synergic muscles responsible for scapulothoracic and glenohumeral joint stability, iii) strength deficit in distal synergic muscles preventing the maintenance of elbow extension by shoulder elbow dynamic coupling, iv) shoulder joint ankyloses, and/or v) shoulder pain. Further studies on open chain movements are needed to identify the contribution of each of these factors in order to tailor upper limb rehabilitation programs for SCI individuals.

Keywords: Tetraplegia, SCI, Upper limb, Reaching, Reach-to-grasp, Kinematic

Cervical spinal cord injury (SCI) leads to extensive sensorimotor deficits affecting both somatic (e.g. upper and lower extremity, trunk) and vegetative functions below the injury level [1]. A C5 SCI preserves innervation of shoulder and elbow flexors while C6 injuries spare wrist extensors and C7 injuries spare elbow extensors in addition (see Table 1). Thus, from a functional perspective, C5 and C6 injuries impair active elbow extension against

gravity while C5 to C7 injuries prevent active grasping [2]. Fortunately, when wrist extension is preserved (i.e. injury at C6 or below), tenodesis can replace active grasp by passive whole hand and lateral grips. During wrist extension tenodesis causes passive tendon shortening of *flexor digitorum superficialis* and *profundus*, leading to passive finger-to-palm flexion, and of *flexor pollicis longus*, leading to thumb-to-index lateral face adduction [3].

Autonomy after tetraplegia is based upon upper limb movements and is achieved by both re-learning open-chain movements like grasping, and learning novel closed-chain movements like manual wheelchair propulsion or sitting pivot transfer. This is achieved by rehabilitation [1,2] and

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Table 1 Upper limb muscles function, innervation [4] and the detail of the consequences of spinal cord injury level on muscle innervation

Joint	Muscles	Function	Innervation		SCI level					
			Nerve	Roots	C4	C5	C6	C7	C8	T1
Shoulder scapulo- thoracic	Serratus anterior	Protraction & upward rotation	Long thoracic	C5 C6 C7	–	±	±	±	+	+
	Trapezius upper part	Elevation	Accessory spinal	XI	+	+	+	+	+	+
	Trapezius middle part	Retraction			+	+	+	+	+	+
	Trapezius lower part	Downward rotation			+	+	+	+	+	+
	Pectoralis minor	Depression & anterior tipping	Medial pectoral	C8 T1	–	–	–	–	±	±
Shoulder gleno- humeral	Deltoïd anterior part & Coracobrachialis	Flexion	Axillary	C5 C6	–	±	±	+	+	+
	Deltoïd medius part	Abduction			–	±	±	+	+	+
	Deltoïd posterior part	Extension			–	±	±	+	+	+
	Pectoralis major upper part	Flexion/Adduction/ Medial rotation	Lateral pectoral	C5 C6 C7	–	±	±	±	+	+
	Pectoralis major middle & lower parts	Flexion/Adduction/ Medial rotation	Medial pectoral	C8 T1	–	–	–	–	±	±
	Lattissimus dorsi	Extension/Adduction/ Medial rotation	Thoracodorsal	C6 C7 C8	–	–	±	±	±	+
	Teres major	Extension/Adduction/ Medial rotation	Subscapularis	C5 C6 C7	–	±	±	±	+	+
	Subscapularis	Medial rotation			–	±	±	±	+	+
	Supraspinatus	Abduction			–	±	±	±	+	+
	Infraspinatus	Lateral rotation			–	±	±	±	+	+
	Teres minor	Lateral rotation	Axillary	C5 C6	–	±	±	+	+	+
Elbow	Biceps brachii	Flexion	Musculo-cutaneous	C5 C6	–	±	±	+	+	+
	Brachialis	Flexion			–	±	±	+	+	+
	Brachioradialis	Flexion			–	±	±	+	+	+
	Triceps brachii	Extension	Radial	C7 C8 T1	–	–	–	±	±	±
Wrist	Extensor carpi radialis longus & brevis	Extension	Radial	C6 C7 C8	–	–	±	±	±	+
	Extensor carpi ulnaris	Extension		C7 C8	–	–	–	±	±	+
	Flexor carpi radialis	Flexion	Median	C6 C7	–	–	±	±	+	+
	Flexor carpi ulnaris	Flexion	Ulnar	C7 C8	–	–	–	±	±	+
Fingers & thumb	Flexor digitorum superficialis	Flexion	Median	C7 C8 T1	–	–	–	±	±	±
	Flexor digitorum profundus	Flexion	Median & ulnar	C8 T1	–	–	–	–	±	±
	Extensor digitorum	Extension	Radial	C6 C7 C8	–	–	±	±	±	+
	Flexor pollicis longus & brevis	Flexion	Median	C8 T1	–	–	–	–	±	±
	Extensor pollicis longus & brevis	Extension	Radial	C7 C8	–	–	–	±	±	+
	Abductor pollicis longus	Abduction			–	–	–	±	±	+
	Abductor pollicis brevis	Abduction	Median	C8 T1	–	–	–	–	±	±
	Opponens pollicis	Opposition			–	–	–	–	±	±
	Adductor pollicis and intrinsic ¹	adduction & ²	Ulnar	C8 T1	–	–	–	–	±	±
	Abductor digitorum minimi	Abduction	Ulnar	T1	–	–	–	–	–	±

¹Intrinsic muscles are lumbricals, palmar and dorsal interossei; ²Functions of previous muscles are flexion of metacarpophalangeal and extension of both proximal and distal interphalangeal joints; adduction and abduction of fingers.

Abbreviation: SCI Spinal Cord Injury.

Muscle innervation depending on level of spinal cord injury was set as minus for non-innervated muscles, plus or minus for partially innervated muscles and plus for normally innervated muscles.

can be complemented by surgical tendon transfer which involves transferring a tendon from a spared muscle (i.e. one with a score above 4/5 at manual muscle testing) to that of a paralyzed muscle [5,6]. If *triceps brachii* is paralyzed, the aim of the surgery is to restore active elbow extension, otherwise its aim is to restore active grasping [7-10].

Clinical assessments are typically used to document upper limb function as well as rehabilitation- or surgery-related improvements [11], but these tests are often subjective and less sensitive than kinematic recordings [12,13]. Thus, to better characterize upper limb movements, kinematic tests have been developed based on reach-to-grasp [14,15], drawing lines [16], overhead movements like shoulder flexion and abduction [17], wheelchair propulsion [18], or sitting pivot transfer [19,20]. Kinematics have also been used to demonstrate intervention-related improvements in upper limb movements after C6 tetraplegia with [21] and without [22] tendon transfer.

Open-chain movements can be programmed and performed in different ways [23]. By examining these movements (that have to be re-learned after injury), SCI provides the opportunity to test theories of motor control [17,24-28], as individuals with SCI should be able to plan movements despite having fewer degrees of freedom to execute them. Although a number of upper limb kinematic studies have been conducted, to date there are no reviews dedicated to addressing the key-features of open-chain movements after cervical SCI. The aim of this paper is to provide such a review, with particular emphasis on the modified kinematics of upper limb movements after tetraplegia.

Methods

We consulted the U.S. National Library of Medicine® (MEDLINE) between 1966 and December 2014. We included full texts from peer-reviewed journals describing kinematics of upper limb movements in alive individuals with complete motor tetraplegia (i.e. AIS scores A and B). We included series case studies of open-chain upper limb movements without extra-load and excluded studies on human cadavers, single cases, and closed-chain upper limb movements.

We examined temporal kinematic parameters including movement time (MT), peak velocity (PV), time to peak velocity (TPV), peaks of acceleration and deceleration, number of PV, acceleration and deceleration peaks. We examined spatial parameters such as trajectory, hand height, joint motion, endpoint accuracy, displacement errors, and joint coordination. We also considered kinematic characteristics after surgery for restoration of elbow extension, and when available, characteristics of physiological recordings e.g. electromyographic activity.

Results

Included articles

We found 24 articles in the database and identified one additional study after reading the references of the 24 articles [29]. We thus examined 25 articles and rejected 7 of these 25 since they did not fulfill at least one of the inclusion criteria: incomplete lesions (AIS D) [16]; single case-study [21,22]; no kinematic recordings [30-32]; human cadavers [33]. The 18 included studies addressed modifications in upper limb motor control during (i) reaching [3,24-27,34-36], (ii) reach-to-grasp [3,14,15,29,35,37] and (iii) overhead movements such as shoulder flexion or abduction [17,38-41]. One study focused on kinematics during fast elbow flexion [28].

Participants

The selected studies included a total of 164 SCI participants with complete motor deficit after injury and 131 healthy controls. Injury level was between C4 and C8. Only one study included high thoracic SCI between T1 and T4 [34] (see Figure 1 and Table 2).

Apparatus

In all studies, the SCI participants sat in their wheelchair while control participants, when included, sat on a standard chair. One study provided no information about trunk stabilization [27], but in all other studies a strap stabilized the chest to the back of the seat except in two studies [34,37] where the trunk had no restriction for anterior motion. Systems used to record 3D motion were electromagnetic, electro-goniometric, optoelectronic, or videographic (see Table 2).

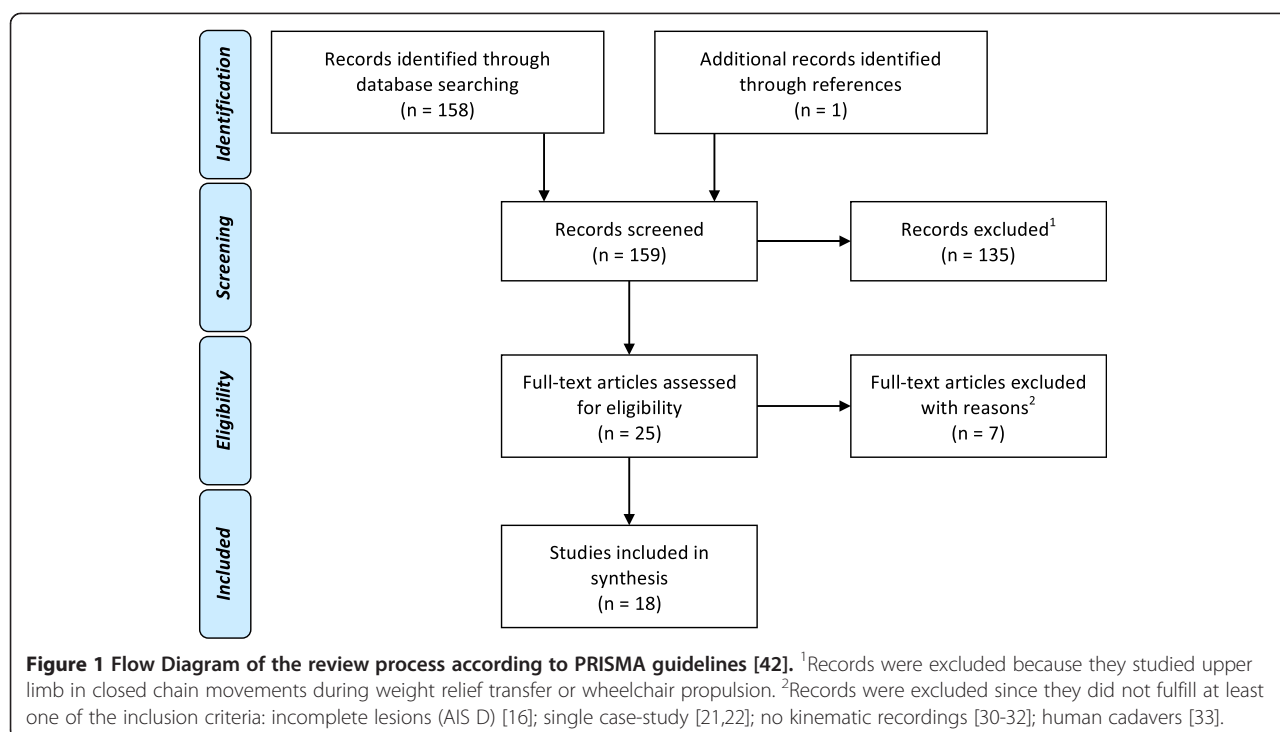
Reaching movements

Temporal kinematics

After C5 to C7 SCI MT increased [3,25-27,35], PV decreased [3,24,26,27,34,35], but TPV was similar to that of control participants [3,26,27]. Compared with control participants, PV was approximately 30% lower and MT more than 40% slower (see Table 3). *After C6 and C7 SCI* the velocity profiles of the hand and fingers remained bell-shaped [3,24,25,35]. *After C6 SCI* variability in PV increased [35], the magnitude of the maximum acceleration and deceleration peaks was reduced and there were multiple acceleration peaks [25] (see Tables 3 and 4).

Spatial kinematics

After C5 to C7 SCI elbow, hand, and finger trajectories remained straight and smooth [25,35]. Movement amplitude with the upper limb fully extended was reduced during maximal reaching in the superior and medial workspace [26]. *After C6 and C7 SCI* the pattern of joint rotation was similar to that of healthy participants [24,25], with an increase in hand height when the target was



placed on the table at elbow height [3,24,35], a decrease in acromion displacement [34,35], and preserved endpoint accuracy [3,24,25,27]. Shoulder and elbow joint motion followed a linear relationship attesting to the preservation of temporal coordination [24,35]. *After C6 SCI* scapula movements increased [35] with more lateral scapula rotation during reaching in the lateral workspace than in healthy participants [24]. Scaling between shoulder and elbow rotation velocity was also preserved [36]. *After C7 SCI* finger trajectory variability increased [34] (see Table 4).

EMG activity

After C6 SCI agonist muscles were not activated in a reciprocal pattern as in healthy individuals. Instead, shoulder muscles were almost exclusively active [25,43], and *pectoralis major* (a shoulder agonist) was active throughout the entire movement, whereas in controls it was active for only part of the movement [25] (see Table 4).

Effect of elbow extension restoration

After tendon transfer in C5 to C7 SCI a slight increase in shoulder flexion and maximal height reached in the superior and medial directions was reported, but these changes did not reach significance [26].

Reach-to-grasp movements

Temporal kinematics

After C6 and C7 SCI MT increased [3,14,35,37] and PV decreased [3,14,29,35]. When compared with control participants, MT was nearly twice as long and PV was

around 11% lower (see Table 3). Due to the longer MT, TPV was delayed [3,14], but occurred earlier than in control participants when normalized to MT [37]. Several studies reported that in SCI participants there was an additional velocity peak between the go and return peaks in the reaching phase [29,35,37]. Interestingly, in one of these studies PV was negatively correlated with ASIA motor index [37]. *After C6 SCI* variability in PV increased [35] and the velocity profile was asymmetric, with a prolonged deceleration phase [3,35]. During reaching before grasping, velocity of shoulder flexion, elbow extension, and wrist tangential velocity were stable (the latter was equal to 20% of its maximum) [15] (see Tables 3 and 5).

Spatial kinematics

After C6-C7 SCI the pattern of joint rotation was similar to that of control participants [14,37], but hand height increased at the end of the reaching phase [3,29,35]. Index finger trajectory variability increased and was negatively correlated with the Functional Independence Measure score [37]. The range of motion at the wrist joint during reaching was greater than in control participants [3,14,29], with the wrist flexed during reaching [3,14,15,29] and extended during grasping and object manipulation [3,14,15,29]. Motion at the shoulder and elbow joints was linearly correlated, attesting to preserved temporal joint coordination [14,29,35], but motion at the shoulder and wrist joints was temporally desynchronized [29]. *After C6 SCI* scapula movements increased during reach to grasp [15,35] while the acromion trajectory was

Table 2 Participant and study characteristics

Authors	Study	SCI level	Patient number	Mean age (years) (range or SD)	Mean delay since injury (months) (range or SD)	Tasks	Kinematic device	EMG recording	Table height	Velocity
Acosta et al.	CC	C5	2	48 (SD 2.6)	NA	Overhead ⁱ	Optotrak™	No	No table	Comfortable
		C6	3							
Cacho et al.	CC	C6	11	30.5 (SD 6.5)	70.9 (SD 44.0)	Grasping ¹	Qualisys™	No	Elbow	Comfortable
		C7	9							
Gronley et al.	SC	C6	15	33 (22 to 44)	108 (36 to 252)	Overhead ⁱⁱ	VICON™	Inv	No table	Comfortable
Hoffmann et al.	SC	C6	9	28.7 (24 to 34)	30.5 (7 to 120)	Grasping ¹	Fastrak™	No	Elbow	Comfortable
		C7	2							
Hoffmann et al.	CC	C6	8	30.4 (24 to 43)	25.4 (5 to 56)	Reaching ^a	Fastrak™	No	Elbow	Comfortable
		C7	7	28.8 (24 to 36)	70.2 (7 to 262)					
Jacquier-Bret et al.	CC	C6	5	39.6 (SD 9.7)	NA	Grasping ²	Flocks of Birds™	Surf	Elbow	Comfortable
Koshland et al.	CC	C6	5	NA (25 to 37)	NA (132 to 216)	Reaching ^b	Videotape recording	Surf	Elbow	Quick
Laffont et al.	SC	C6	4	29 (26 to 34)	10 (5 to 19)	Reaching ^{c,d}	Fastrak™	No	Elbow	Comfortable
						Grasping ¹				
Maksimovic et al.	CC	C4	2	33.1 (3 to 60)	68.7 (12 to 144)	Overhead ⁱⁱⁱ	Goniometer	No	No table	Comfortable
		C5	2							
		C6	5							
		C7	7							
Mateo et al.	CC	C6	4	27.5 (SD 8.3)	68 (6 to 216)	Reaching ^c	VICON™	No	Elbow	Comfortable
						Grasping ^{3,4}				
Nunome et al.	CC	C7	5	32.6 (SD 2.4)	NA (108 to 252)	Basketball throw	Videotape recording	No	No table	Comfortable
		C8	1							
Popovic et Popovic	CC	C6	6	NA	NA	Reaching ^d	Goniometer	No	Shoulder	Comfortable
Robinson, Barton et al.	CC	C5	2	42.8 (SD 12.1)	183.3 (SD 126.9)	Reaching ^e	Qualisys™	No	No table	Comfortable
		C6	8							
		C7	1							
Robinson, Hayes et al.	CC	C6	5	39 (SD 9)	211.2 (SD 60.4)	Reaching ^f	Qualisys™	No	Elbow	Quick
Reft et hasan	CC	C7	1	25.8 (23 to 35)	NA (36 to 92)	Reaching ^g	Selspot™	No	No table	Quick
		T1 and T2	2							
		T4	2							
Remy-Neris et al.	CC	C6	5	27.0 (SD 6.0)	Chronic SCI	Overhead ^{iv}	VICON™	No	No table	Comfortable
Reyes-Guzman et al.	CC	C6	8	33.6 (SD 13.0)	8.5 (SD 2.2)	Grasping ⁵	Codamotion™	No	Elbow	Comfortable
		C7	8	28.8 (SD 9.8)	7.5 (SD 1.9)					
Wierzbicka et al.	CC	C5	7	40 (21 to 64)	149.3 (3.6 to 432)	Elbow flexion	Homemade	Surf	Shoulder	Quick

Reaching: ^awith a pointer fixed at dorsum of the hand; ^bwith arm rolling on table and wrist splinted; ^ctarget on the table; ^dobject non specified; ^etargets at 5 locations of reachable space; ^fhand rolling over table with frictionless system; ^g2 targets set at ipsilateral shoulder level.

Grasping: ¹a cone; ²a low mass cubic object; ³apple; ⁴vertical floppy disk; ⁵a glass.

Overhead movements: ⁱShoulder flexion, abduction in frontal plane and in scapula plane with elbow extended; ⁱⁱShoulder flexion and abduction and 4 ADL (consisting in drinking from an empty cup, flipping a lightswitch, hair combing, and reaching for the perineum.); ⁱⁱⁱShoulder flexion and abduction; ^{iv}Shoulder flexion with elbow extended or hand to nape of the neck.

Abbreviations: SCI Spinal cord injury, NA not available, SC series case, CC control case, ADL activity of daily life, Inv invasive, Surf surface.

Table 3 Review of movement time and velocity peak in SCI and control participants

Authors	Tasks	Distance (cm)	PV (m/s)			MT (s)		
			SCI	Control	SCI/control (%)	SCI	Control	SCI/control (%)
Hoffmann et al.	R	Arm length	0.87 ± 0.04	1.00 ± 0.04	13.00	NA	NA	NA
Koshland et al.	R	20	0.60 ^a	1.30	53.85	NA	NA	NA
Laffont et al.	R	Low	0.83 ± 0.25	1.08 ± 0.31	23.15	NA	NA	NA
		High	1.10 ± 0.31	1.47 ± 0.25	25.17			
Mateo et al.	R	28 ^b	0.66 ± 0.17	0.94 ± 0.22	29.79	0.66 ± 0.20	0.44 ± 0.14	50.00
			0.78 ± 0.19	1.15 ± 0.25	32.17	0.67 ± 0.24	0.47 ± 0.14	42.55
Popovic et Popovic	R	NA	NA	NA	NA	NA	NA	NA
Reft et Hasan	R	Far no support	0.35 ± 0.07	0.50 ± 0.09	30.10	NA	NA	NA
		Far support	0.32 ± 0.04	0.48 ± 0.07	33.19			
Robinson, Barton et al.	R	Arm length	NA ^c	NA ^c	NA	NA ^c	NA ^c	NA
Robinson, Hayes et al.	R	20	0.59	0.92	35.87	0.67	0.49	36.73
Cacho et al.	G	Arm length	0.79 ± 0.14	0.88 ± 0.14	10.23	1.53 ± 0.08	0.92 ± 0.16	66.3
Hoffmann et al.	G	Arm length	1.07 ± 0.05	1.22 ± 0.06	12.3	NA ^d	NA ^d	NA
Jacquier-Bret et al.	G	40	0.7 ^e	0.9 ^e	22.22	NA ^c	NA ^c	NA
Laffont et al.	G	Short	0.92 ± 0.25	1.08 ± 0.31	14.81	3.12 ± 0.85	1.81 ± 0.45	72.38
		Long	1.04 ± 0.28	1.19 ± 0.31	12.61	3.30 ± 1.08	1.82 ± 0.25	81.32
Mateo et al.	G	35	0.71 ± 0.13	0.80 ± 0.08	11.25	1.90 ± 0.60	0.77 ± 0.09	146.75
			0.67 ± 0.09	0.69 ± 0.08	2.90	1.64 ± 0.13	0.75 ± 0.12	118.67
Reyes-Guzman et al.	G	18	0.56 ± 0.26 ^f	0.66 ± 0.09	15.15	2.57 ± 0.98 ^f	1.04 ± 0.33	147.12
			0.67 ± 0.53 ^g		-1.52	1.66 ± 1.07 ^g		59.62
Acosta et al.	O	NA	NA	NA	NA	NA	NA	NA
Gronley et al.	O	NA	NA	NA	NA	NA	NA	NA
Maksimovic et al.	O	NA	NA	NA	NA	0.65 ± 0.17	0.45	44.44
Nunome et al.	O	2.16	4.26 ± 0.67 ^h	5.45 ± 0.25 ^h	21.83	NA	NA	NA
Remy-Neris et al.	O	NA	62 ± 22 ⁱ	201 ± 41 ⁱ	69.15	NA	NA	NA
			109 ± 39 ⁱⁱ	241 ± 29 ⁱⁱ	54.77			
Wierzbicka et al.	E	NA	NA	NA	50	twice control	NA	200

^aFor n = 4 SCI, only one exhibit 1.1 m/s velocity; ^bTargets were placed centrally or laterally on the right; ^cNon significant differences were reported without data available.

^dIncrease time between end of reaching and grasping in SCI participants; ^eValue rounded extracted from figure; ^fValue for C6 SCI participants; ^gValue for C7 SCI participants; ^hVertical component of basketball after shooting; ⁱMaximal shoulder flexion and ⁱⁱmaximal elbow flexion both expressed in degree per seconds in italics.

Abbreviations: NA Not Available, P Pointing, G Grasping, O Overhead, E Elbow flexion.

MT Movement Time, PV Velocity Peak; cm centimeter, m/s meter per seconds, s seconds.

shorter and less linear [35]. During tenodesis, wrist extension angle was greater for lateral than whole hand grip [3] (see Table 5).

EMG activity

After C6 SCI contraction of the agonists increased but contrary to healthy participants this increase was not paralleled by increased contraction in the antagonists [15] (see Table 5).

Overhead movements

Temporal kinematic

After C6 SCI MT increased and shoulder velocity decreased [17]. After C6 to C8 SCI wrist flexion velocity decreased

[40] while elbow velocity remained unchanged [17,40]. PV was almost half that of control participants, and MT nearly one and a half times slower (see Tables 3 and 6).

Spatial kinematics

After C5 to C7 SCI participants presented less linear in hand trajectory and larger shoulder and elbow joint rotations than healthy controls [39]. After C5 to C8 SCI active shoulder flexion angle decreased while abduction angle increased compared with healthy controls [17,40,41]. After C5 and C6 SCI, the scapula was located more medially and exhibited 'winging' i.e. protrusion of the lower and medial parts from the thorax in the resting position. During shoulder flexion, there was less lateral rotation of

Table 4 Kinematic characteristics of reaching movements after tetraplegia

Parameters		Main results	SCI motor level			References
			C5	C6	C7	
Movement time (MT)	T	Increased	X	X	X	[3,25-27,35]
Velocity Peak (PV)	T	Decreased	X	X	X	[3,24,26,27,34,35]
		Variability increased		X		[35]
Acc & dec peaks	T	Reduced magnitude		X		[25]
Number of acc peaks	T	Multiple		X		[25]
Time to Velocity Peak (TPV)	T	Similar to control	X	X	X	[3,26,27]
Velocity profile ¹	T	Bell-shaped		X	X	[3,24,25,35]
Velocity coordination	T	Shoulder velocity equal to half of elbow velocity		X		[36]
Trajectory ²	S	Straight and smooth		X	X	[25,35]
		Variability increased			X	[34]
Hand height	S	Not increased		X	X	[3,24,35]
Joint motion	S	Similar pattern of joint rotation		X	X	[24,25]
		Increased of scapula movement		X		[35]
		Decreased of sup and med max reaching	X	X	X	[26]
		Decreased of acromion displacement		X	X	[34,35]
Endpoint accuracy	S	Preserved		X	X	[3,24,25,27]
Joint coordination ³	S	Linear temporal relationship		X	X	[24,35]
EMG activity	N	Activation of agonist without antagonist muscles		X		[25]
		Selective activation of shoulder muscles		X		[25]
		Prolonged muscle activation		X		[25]

¹of hand and finger; ²of elbow, hand and finger; ³of shoulder and elbow.

Abbreviations: T Temporal kinematic parameter, S Spatial kinematic parameter, N Non kinematic parameter, acc acceleration, dec deceleration, max maximal, sup superior, med medial.

the scapula for SCI individuals compared with controls [41]. After C6 SCI passive range of motion decreased during shoulder flexion (133°, SD = 9°) and abduction (133°, SD = 10°) [38] compared with healthy individuals (flexion = 156°, SD = 9° and abduction = 161°, SD = 11°) [44]. Movements of the glenohumeral joint were linearly related to both elbow and scapulothoracic joint movements attesting to preservation of temporal coupling [17,41]. After C7 and C8 SCI, forward and upward displacement of the shoulder increased [40] (see Table 6).

EMG activity

After C6 SCI shoulder and elbow maximal isometric strength decreased [38]. Shoulder internal and external rotator strength decreased by 67% and 39% of control capacity, respectively [38], and contraction intensity increased [38] (see Table 6).

Effect of elbow extension restoration

Elbow extension restoration after C6 SCI altered kinematics towards patterns observed in control participants as it reduced prolonged MTs [17], and increased shoulder flexion angle, which in turn decreased shoulder abduction angle and scapula lateral rotation [17] (see Table 6).

Effects of extensor impairment on elbow flexion

Only one study analyzed the accuracy of fast, single-joint elbow flexion of either 10°, 20° or 30° with and without a constant extensor torque provided by a manipulandum [28]. After C5 SCI the maximal isometric strength of elbow flexors was about 50% of controls (mean 46.3 Nm versus 78 Nm). Without elbow extensor torque, movements were smooth but slower than in controls, and there were more errors. In contrast, movement velocity increased and errors decreased when elbow extensor torque was provided.

General discussion

Individuals with SCI can relearn open-chain movements despite reduced degrees of freedom and even though the kinematics of these movements differ from those of normal controls they preserve several kinematic invariants like movement endpoint accuracy and minimal cost.

Partial motor preservation after SCI

Markers placed on either the fingers, wrist, elbow or acromion revealed preserved trajectories after C5 to C8 SCI during both reaching and reach-to-grasp [24,25,28,35], attesting to the fact that SCI participants can produce efficient smooth trajectories similar to

Table 5 Kinematic characteristics of reach-to-grasping movements after tetraplegia

Parameters		Main results	SCI motor level			References
			C5	C6	C7	
Movement time (MT)	T	Increased		X	X	[3,14,35,37]
Velocity Peak (PV)	T	Decreased		X	X	[3,14,29,35]
		Variability increased		X		[35]
		Negative correlation with ASIA score		X	X	[37]
Time to PV (TPV)	T	Delayed time to PV		X	X	[3,14,37]
Number of PV	T	Two peaks (reaching and return)		X	X	[29,35]
		Additional PV (grasping)		X	X	[29,35,37]
Velocity	T	Stable ¹ before grasping		X		[15]
Velocity profile ²	T	Asymmetric with a prolonged decelerative phase		X		[3,35]
Trajectory ³	S	Straight and smooth		X		[35]
Trajectory ⁴	S	Reduced and less straight		X		[35]
Trajectory ⁵	S	Increased curvature index		X	X	[37]
Trajectory ⁶	S	Negative correlation with FIM		X	X	[37]
Hand height	S	Increased at the end of the reaching phase		X	X	[3,29,35]
Joint motion	S	Similar pattern of joint rotation		X	X	[14,37]
		Increased of scapula movement		X		[15,35]
		Increased wrist flexion/extension range of motion		X	X	[3,14,29]
		Wrist flexion during reaching		X	X	[3,14,15,29]
		Wrist extension for grasping and manipulating		X	X	[3,14,15,29]
Joint coordination ⁷	S	Increased of wrist extension for LG vs WHG		X		[3]
		Temporal linear relationship		X	X	[14,29,35]
		Temporal decoupling		X	X	[29]
		Increased		X		[15]
		Activation of agonist without antagonist muscle		X		[15]

¹for shoulder flexion, elbow extension and wrist tangential velocity; ²of hand and finger; ³of elbow, hand and finger; ⁴of acromion; ⁵of wrist; ⁶of index; ⁷of shoulder and elbow; ⁸of shoulder and wrist; ^a2002.

Abbreviations: T Temporal kinematic parameter, S Spatial kinematic parameter, N Non kinematic parameter, PV Velocity Peak, FIM Functional Independence Measure, LG Lateral Grip, WHG Whole Hand Grip.

controls during reaching [25,35] and reaching-to-grasp [35]. TPV and the shape of the velocity profiles [3,26,27] along with reaching accuracy (attesting to endpoint accuracy [3,24,25,27]) were comparable with controls during reaching but not during reach-to-grasp and overhead movements. Indeed, motor control after SCI is characterized by strong kinematic invariants like movement endpoint accuracy and movement cost reduction as attested by the smooth trajectories and bell-shaped velocity profiles [45]. The relative preservation of these kinematic features is due to compensatory mechanisms, in particular during grasping and overhead movements as developed below.

Shoulder and elbow coordination after SCI

Notwithstanding the overall reduction of degrees of freedom for the upper limb, SCI individuals show patterns of shoulder and elbow coordination similar to healthy individuals during reaching and reach-to-grasp [14,24,25,39].

That is, the linear temporal relationship [24,35] and the velocity coupling [36] between these joints are preserved, but at the cost of other reorganizational changes. The main change occurs at the scapulothoracic joint, where scapula rotation increases during reaching [35] and reach-to-grasp [15,35], and both upward and external scapula rotations increase [15,40] in order to orient and stretch out the upper limb [24]. A complementary change occurs at the glenohumeral joint, where increased abduction mitigates the reduced flexion during overhead movements [17]. These scapulothoracic and glenohumeral joint compensatory movements ensure that mechanical dynamic interactions between the shoulder and elbow produce elbow extension despite *triceps brachii* paralysis [24].

Reduction of the upper limb workspace after SCI

SCI leads to extensive sensorimotor deficits, for example, strength loss due to partial innervation (see Table 1) which leads to a decrease in full shoulder active range of motion

Table 6 Kinematic characteristics of overhead upper limb movements

Parameters		Main results	SCI motor level				References
			C5	C6	C7	C8	
Movement time (MT)	T	Increased		X			[17]
Velocity	T	Decreased at shoulder joint		X			[17]
Velocity	T	No differences at elbow joint		X	X	X	[17,40]
Velocity	T	Decreased for wrist flexion		X	X	X	[40]
Trajectory ¹	S	Variability increased	X	X	X		[39]
Joint motion	S	Similar pattern of joint rotation	X	X	X		[39]
		Pattern of joint rotation variability increased	X	X	X		[38,39]
		Decreased shoulder flexion and increased abduction	X	X	X	X	[17,40,41]
		Increased upward and forward shoulder motion			X	X	[40]
		Winging ² and adducted scapula during rest	X	X			[41]
		Decreased scapula lateral rotation during shoulder flexion	X	X			[41]
		Increased elbow flexion		X			[17]
		Temporal linear relationship	X	X			[17,41]
		Decreased strength for shoulder rotator and elbow flexors		X			[28,38]
EMG activity	N	Increased contraction intensity for same task		X			[38]
		Reduced movement duration		X			[17]
Effect of elbow extension restoration	T	Increased shoulder joint velocity		X			[17]
	S	Increased shoulder flexion and decreased abduction		X			[17]
	S	Decreased elbow flexion		X			[17]

¹of the hand; ²lower and medial part rotated outwards from the thorax ³between glenohumeral and scapulothoracic joints, ⁴between glenohumeral and elbow joints.

Abbreviations: T Temporal kinematic parameter, S Spatial kinematic parameter, N Non kinematic parameter.

(i.e. reduced shoulder flexion and abduction angles [17,38,41]) and a reduction of scapula lateral rotation [41]. Several complementary hypotheses have been put forward to account for the reduction of the superior and superiomedial reaching workspace in C5 and C6 SCI individuals. One idea is that a strength deficit in the glenohumeral joint agonist could perturb these movements. Indeed, partial denervation of the *pectoralis major* (normal innervation C5-T1) results in decreased strength of the primary humeral adductor [26]. Increased EMG contraction intensity after SCI [38] might be a marker of the difficulty associated with these movements. A second idea is that a proximal deficit in *serratus anterior* (normal innervation C5-C7) means that this muscle cannot resist against the tension of the *rhomboids* antagonist muscles (normal innervation C4-C5) which results in both a reduction in scapula lateral rotation and in scapulothoracic instability. This could decrease the shoulder's full active range of motion [41]. A third idea is that a distal deficit of the *triceps brachii* (normal innervation C7-T1) [26] might force C5-C6 SCI individuals to reduce overhead workspace in order to keep the elbow extended and to maintain the mechanical dynamic interaction between the shoulder and elbow. Fourth, shoulder ankylosis could reduce superiomedial and superior reach by reducing

passive full range of motion by about 25° during both shoulder flexion and abduction compared with healthy individuals [38,44]. A final factor is shoulder pain, which is reported by more than half of the individuals with tetraplegia [46], and probably contributes to the functional limitation of the workspace.

Main temporal kinematic difference after SCI: prolonged movement time

The main consequence of SCI is increased MT [3,14,17,25,28,35] which is associated with decreased PV [3,14,24,28,29,35]. Acceleration and deceleration peaks are lower during reaching [25] and shoulder velocity decreases during overhead movements [17]. Motor slowing might be due to shoulder and elbow muscle strength decreases [28,38], as SCI participants with weaker preserved upper limb muscles exhibit lower velocity and acceleration peaks and increased MTs. Importantly, motor slowing could also be due to *triceps brachii* paralysis which prevents agonist-antagonist co-contraction, which is observed in healthy individuals and serves to stop movement [25,43]. Indeed, elbow flexion velocity decreases when *triceps brachii* is paralyzed but can be increased when a manipulandum provides a constant extensor torque [28]. Moreover, elbow stiffness due to impairment

of agonist–antagonist co-contraction probably contributes to the alteration of reaching movements [24]. According to Fitt's law and the speed-accuracy trade-off principle, motor slowing could reflect central adaptation to maintain accuracy at levels similar to those of healthy individuals [47]. This is consistent with the observation of reduced accuracy during fast elbow flexion movements [28]. Furthermore, grasping is the main cause of increased MT [29], as MT is nearly twice that of controls during grasping but only one and a half times longer during reaching and overhead movements (see Table 3). It is noteworthy that the reduction of MT is not related to the need to avoid trunk imbalance since trunk support did not increase velocity during fast upper limb movements [34].

Requirements of grasping

Transport phase

Jeannerod described the transport and grasping phases of reach-to-grasp [48] and studies of the former phase classically used reaching movements. SCI and healthy individuals exhibit similar reaching movements, which favors the partial motor compensation previously discussed. Kinematic differences appear during grasping, however, with prolonged deceleration of the transport phase as attested by (i) delayed TPV [3,14,37], (ii) asymmetric velocity profile of both the hand and fingers [3,35], and (iii) stable shoulder flexion, elbow extension and wrist tangential velocity before grasping [15]. These differences reflect the modification of the duration of the transport and grasping phases as the transport phase is initially quick but slows down towards the end [48]. Indeed, after SCI the transport phase of reach-to-grasp is characterized by reduced acceleration and prolonged deceleration durations, favoring final hand adjustment and successful grip. Finally, maximal grip aperture, a sign of grip preparation during transport [48], is lost because of finger extensor paralysis. Since grip aperture is passive and relies on wrist flexion and elbow pronation (favoring finger opening with gravity), grip preparation is effective only if the size of the object to be grasped is less than the maximal achievable grip width.

Grasping phase: tenodesis grasp

Wrist extension is a key-component of tenodesis grasp [3,14,15,29]. Indeed, wrist extension and tendon shortening [3] lead to two passive grips: whole hand and lateral grip. In SCI participants wrist extension is greater during lateral than whole hand grip, suggesting a greater need for tendon shortening during lateral grip [3]. Increased hand height during reach-to-grasp brings the hand above the object thus preventing collision, and could explain EMG contraction intensity increases [15]. Joint coupling during tenodesis grasping is different from that observed in healthy individuals. Specifically, SCI individuals plan

transport and grasping phases consecutively and the second velocity peak during grasping demonstrate a second movement following reaching [29,35]. The negative correlation between the number of velocity peaks and the ASIA motor index indicates that the higher the SCI level the more fragmented the movement [37]. Finally, reaching and grasping are successively planned after C6-C7 SCI as attested by the wrist flexion during transport but the wrist extension during grasping [3,14,15,29], and the loss of temporal coupling between the shoulder and wrist during reach-to-grasp [15]. This contrasts with normal reach-to-grasp where the grip is prepared during the transport phase [48].

Effect of elbow extension restoration

Restoration of elbow extension, either by tendon transfer surgery from *posterior deltoid* to *triceps brachii* [17,26] or the use of a manipulandum that provides an extensor torque [28], decreases MT [17,26,28] and reduces errors [28]. This is due to the restoration of elbow stiffness which in turn decreases the need for glenohumeral compensatory movements during overhead movements. Specifically, the shoulder abduction angle decreases favoring flexion [17] while the shoulder joint velocity concomitantly increases [17]. Surgery also improves strength and general performance, and participants report high satisfaction after their operations [49]. Although functional improvements are reported, surgery fails to completely restore motor function [50] as shown by the absence of improvements during both superior and medial maximal reaching [26].

Conclusion

SCI participants efficiently execute a broad range of upper limb tasks. Kinematic evidence shows that, even after SCI, movements are planned and executed according to strong kinematic invariants like movement endpoint accuracy and minimal cost. Elbow extension with a weak or paralyzed *triceps brachii* relies on increased movements of the scapulothoracic and glenohumeral joints. This provides a dynamic coupling between the shoulder and elbow which palliates the *triceps brachii* paralysis but limits the superior maximal reach. Moreover, reach-to-grasp planning is modified with reaching and grasping performed successively contrary to normal grasping patterns where grasping is prepared during the transport phase. The prolonged transport phase ensures correct hand placement while the grasping relies on wrist extension eliciting either whole hand or lateral grip. One main kinematic characteristic after tetraplegia is motor slowing attested by increased MT which can be a direct consequence of the strength deficit or due to a behavioral adaptation in order to preserve the accuracy of the movement and ensure grasping by tenodesis. Another issue concerns the reduction of maximal superior reaching during

overhead movements. This can be caused by a strength deficit of either shoulder agonist or synergic muscles along with shoulder ankylosis and pain. Moreover, increased shoulder movements could favor shoulder pain, especially since this joint is already under severe strain. This could promote shoulder overuse pathologies which lead to pain and ankylosis, which then further contribute to the impairment. Indeed, further studies on open chain movements are needed to identify the contribution of each of these previous reasons in order to tailor upper limb rehabilitation programs for SCI individuals.

Abbreviations

SCI: Spinal cord injury; C5/6/7/8 and T1/2: Cervical and thoracic vertebra indicating the level of spinal cord injury; ASIA: American Spinal Injury Association; AIS: ASIA Impairment Scale; US: United States of America; MT: Movement time; PV: Peak velocity; TPV: Time to peak velocity; EMG: Electromyogram; Nm: Newton per meter.

Competing interests

The authors declare that they have no competing interests.

Authors' contributions

SM addressed the electronic database MEDLINE. Then, SM ARB YR and GR analysis and interpret the data. SM drafting the manuscript and ARB YR GR and CC revised it critically. All authors read and approved the final manuscript.

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References

- Long C, Lawton E. Functional significance of spinal cord lesion level. *Arch Phys Med Rehabil*. 1955;36:249–55.
- Woolsey R. Rehabilitation outcome following spinal cord injury. *Arch Neurol*. 1985;42:116–9.
- Mateo S, Revol P, Fournass M, Rossetti Y, Collet C, Rode G. Kinematic characteristics of tenodesis grasp in C6 quadriplegia. *Spinal Cord*. 2013;51:144–9.
- Chevalier A-M, Miranda A, Lacôte M, Bleton JP. Clinical evaluation of muscle function. Michigan: Churchill Livingstone; 1987.
- Moberg E. Surgical rehabilitation of the upper limb in tetraplegia. *Paraplegia*. 1990;28:330–4.
- McDowell CL, Moberg E, House JH. The second international conference on surgical rehabilitation of the upper limb in tetraplegia (quadriplegia). *J Hand Surg*. 1986;11:604–8.
- Freehafer A, Alvin A. Gaining independence in tetraplegia. Cleveland technique. *Clin Orthop Relat Res*. 1988;355:282–9.
- Lamb DW, Landry R. The hand in quadriplegia. *Hand*. 1971;3:31–7.
- Lamb DW, Chan KM. Surgical reconstruction of the upper limb in traumatic tetraplegia. A review of 41 patients. *J Bone Joint Surg (Br)*. 1983;65:291–8.
- Vanden Berghe A, Van Laere M, Hellings S, Vercauteren M. Reconstruction of the upper extremity in tetraplegia: functional assessment, surgical procedures and rehabilitation. *Paraplegia*. 1991;29:103–12.
- Mulcahey MJ, Hutchinson D, Kozin S. Assessment of upper limb in tetraplegia: considerations in evaluation and outcomes research. *J Rehabil Res Dev*. 2007;44:91–102.
- Bernhardt J, Bate PJ, Matyas TA. Accuracy of Observational Kinematic Assessment of Upper-Limb Movements. *Phys Ther*. 1998;78:259–70.
- Van Dokkum L, Hauret I, Mottet D, Froger J, Metrot J, Laffont I. The Contribution of kinematics in the assessment of upper limb motor recovery early after stroke. *Neurorehabil Neural Repair*. 2014;28:4–12.
- De los Reyes-Guzman A, Gil-Agudo A, Penasco-Martin B, Solis-Mozos M, del Ama-Espinosa A, Perez-Rizo E. Kinematic analysis of the daily activity of drinking from a glass in a population with cervical spinal cord injury. *J Neuroeng Rehabil*. 2010;7:41–52.
- Jacquier-Bret J, Rezzoug N, Vallier JM, Tournebise H, Gorce P. Reach to grasp kinematics and EMG analysis of C6 quadriplegic subjects. *Conf Proc IEEE Eng Med Biol Soc*. 2009;2009:5934–7.
- Van der Linde H, Snoek G, Guerts A, van Limbeek J, Mulder T. Kinematic assessment of manual skill following functional hand surgery in tetraplegia. *J Hand Surg*. 2000;25:1146–6.
- Remy-Neris O, Milcamps J, Chikhi-Keromest R, Thevenon A, Bouttens D, Bouilland S. Improved kinematics of unrestrained arm raising in C5–C6 tetraplegic subjects after deltoid-to-triceps transfer. *Spinal Cord*. 2003;41:435–45.
- Gil-Agudo A, Del Ama-Espinosa A, Pérez-Rizo E, Pérez-Nombela S, Pablo R-RL. Upper limb joint kinetics during manual wheelchair propulsion in patients with different levels of spinal cord injury. *J Biomech*. 2010;43:2508–15.
- Gagnon D, Nadeau S, Gravel D, Noreau L, Larivière C, Gagnon D. Biomechanical analysis of a posterior transfer maneuver on a level surface in individuals with high and low-level spinal cord injuries. *Clin Biomech*. 2003;18:319–31.
- Desroches G, Vermette M, Gourdou P, Gagnon D. Development of an automated method to detect sitting pivot transfer phases using biomechanical variables: toward a standardized method. *J Neuroeng Rehabil*. 2012;9:7.
- Grangeon M, Guillot A, Sancho P-O, Picot M, Revol P, Rode G, et al. Rehabilitation of the elbow extension with motor imagery in a patient with quadriplegia after tendon transfer. *Arch Phys Med Rehabil*. 2010;91:1143–6.
- Grangeon M, Revol P, Guillot A, Rode G, Collet C. Could motor imagery be effective in upper limb rehabilitation of individuals with spinal cord injury? A case study. *Spinal Cord*. 2012;50:766–71.
- Bernstein N. *The Co-Ordination and Regulation of Movements*. New York: Pergamon Press Ltd.; 1967.
- Hoffmann G, Laffont I, Hanneton S, Roby-Brami A. How to extend the elbow with a weak or paralyzed triceps: Control of arm kinematics for aiming in C6–C7 quadriplegic patients. *Neuroscience*. 2006;139:749–65.
- Koshland GF, Galloway JC, Farley B. Novel muscle patterns for reaching after cervical spinal cord injury: a case for motor redundancy. *Exp Brain Res*. 2005;164:133–47.
- Robinson MA, Barton GJ, Lees A, Sett P. Analysis of tetraplegic reaching in their 3D workspace following posterior deltoid-triceps tendon transfer. *Spinal Cord*. 2010;48:619–27.
- Robinson MA, Hayes SJ, Bennett SJ, Barton GJ, Elliott D. Sensory-motor equivalence: manual aiming in C6 tetraplegics following musculotendinous transfer surgery at the elbow. *Exp Brain Res*. 2010;206:81–91.
- Wierzbicka MM, Wiegner AW. Effects of weak antagonist on fast elbow flexion movements in man. *Exp Brain Res*. 1992;91:509–19.
- Hoffmann G, Laffont I, Roby-Brami A. Co-ordination of reaching movements in patients with cervical spinal cord injury. *Curr Psychol Cognit*. 2002;21:305–40.
- Au AT, Kirsch RF. EMG-based prediction of shoulder and elbow kinematics in able-bodied and spinal cord injured individuals. *IEEE Trans Rehabil Eng*. 2000;8:471–80.
- Laffont I, Hoffmann G, Dizien O, Revol M, Roby-Brami A. How do C6/C7 tetraplegic patients grasp balls of different sizes and weights? Impact of surgical musculo-tendinous transfers. *Spinal Cord*. 2007;45:502–12.
- Wierzbicka MM, Wiegner AW. Accuracy of motor responses in subjects with and without control of antagonist muscle. *J Neurophysiol*. 1996;75:2533–41.
- Muzykewicz DA, Arnet UA, Lieber RL, Fridén J. Intrinsic hand muscle function, part 2: kinematic comparison of 2 reconstructive procedures. *J Hand Surg*. 2013;38:2100–5.
- Reft J, Hasan Z. Trajectories of target reaching arm movements in individuals with spinal cord injury: effect of external trunk support. *Spinal Cord*. 2002;40:186–91.

35. Laffont I, Briand E, Dizien O, Combeaud M, Bussel B, Revol M, et al. Kinematics of prehension and pointing movements in C6 quadriplegic patients. *Spinal Cord*. 2000;38:354–62.
36. Popović M, Popović D. A new approach to reaching control for tetraplegic subjects. *J Electromyogr Kinesiol*. 1994;4:242–53.
37. Cacho EWA, de Oliveira R, Ortolan RL, Varoto R, Cliquet A. Upper limb assessment in tetraplegia: clinical, functional and kinematic correlations. *Int J Rehabil Res*. 2011;34:65–72.
38. Gronley JK, Newsam CJ, Mulroy SJ, Rao SS, Perry J, Helm M. Electromyographic and kinematic analysis of the shoulder during four activities of daily living in men with C6 tetraplegia. *J Rehabil Res Dev*. 2000;37:423–32.
39. Maksimovic R, Popovic M. Classification of tetraplegics through automatic movement evaluation. *Med Eng Phys*. 1999;21:313–27.
40. Nunome H, Doyo W, Aaltonen S, Ikegami Y, Yabe K. A kinematic study of the upper-limb motion of wheelchair basketball shooting in tetraplegic adults. *J Rehabil Res Dev*. 2002;39:63–72.
41. Acosta AM, Kirsch RF, van der Helm FCT. Three-dimensional shoulder kinematics in individuals with C5-C6 spinal cord injury. *Proc Inst Mech Eng H*. 2001;215:299–307.
42. Moher D, Liberati A, Tetzlaff J, Altman DG, PRISMA Group. Preferred reporting items for systematic reviews and meta-analyses: the PRISMA statement. *PLoS Med*. 2009;6:e1000097.
43. Adamovich SV, Levin MF, Feldman AG. Central modifications of reflex parameters may underlie the fastest arm movements. *J Neurophysiol*. 1997;77:1460–9.
44. Kolber MJ, Hanney WJ. The reliability and concurrent validity of shoulder mobility measurements using a digital inclinometer and goniometer: a technical report. *Int J Sports Phys Ther*. 2012;7:306–13.
45. Todorov E. Optimality principles in sensorimotor control. *Nat Neurosci*. 2004;7:907–15.
46. Pahys JM, Mulcahey MJ, Hutchinson D, Betz RR. Scapular stabilization in patients with spinal cord injury. *J Spinal Cord Med*. 2009;32:389–97.
47. Fitts PM. The information capacity of the human motor system in controlling the amplitude of movement. *J Exp Psychol*. 1954;47:381–91.
48. Jeannerod M. The timing of natural prehension movements. *J Mot Behav*. 1984;16:235–54.
49. Kozin SH, D'Addesi L, Chafetz RS, Ashworth S, Mulcahey MJ. Biceps-to-triceps transfer for elbow extension in persons with Tetraplegia. *J Hand Surg*. 2010;35:968–75.
50. Fridén J, Lieber RL. Quantitative evaluation of the posterior deltoid to triceps tendon transfer based on muscle architectural properties. *J Hand Surg*. 2001;26:147–55.

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